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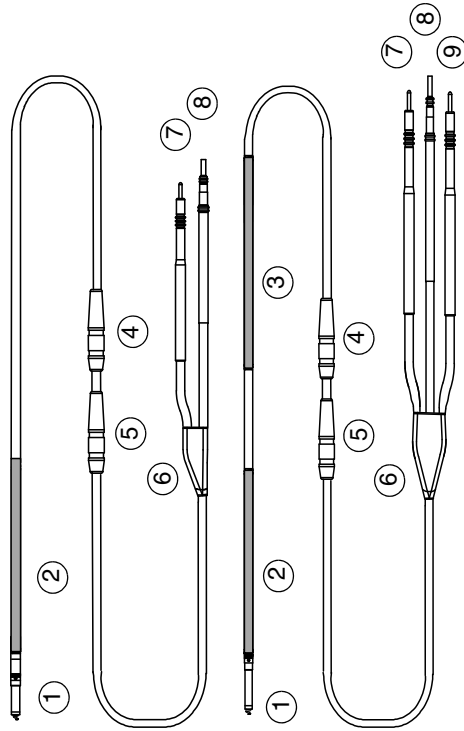
PHYSICIAN'S LEAD MANUAL

ENDOTAK RELIANCE[®] G
ENDOTAK RELIANCE[®] SG

**Steroid-Eluting
Extendable/Retractable Helix Defibrillation Leads**

MODEL 0184/0185/0186/0187
0180/0181/0182/0183

RESTRICTED DEVICE: Federal
law (USA) restricts the sale,
distribution, or use of this device
to, by, or on the lawful order of a
physician.



ENDOTAK RELIANCE® SG Lead,
Models 0180/0181/0182/0183

ENDOTAK RELIANCE® G Lead,
Models 0184/0185/0186/0187

1. Distal steroid-eluting pace/sense electrode (cathode)
2. Proximal pace/sense coil electrode (anode), distal defibrillating coil electrode
3. Proximal defibrillating coil electrode—ENDOTAK RELIANCE G only
4. Suture Sleeve
5. Second Suture Sleeve—Models 0183 and 0187 only
6. Yoke
7. Distal defibrillating electrode terminal (cathode)
8. Proximal and distal pace/sense electrode terminal
9. Proximal defibrillating electrode terminal (anode) ENDO-TAK RELIANCE G only

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Boston Scientific Corporation acquired Guidant Corporation in April 2006. During our transition period, you may see both the Boston Scientific and Guidant names on product and patient materials. As we work through the transition, we will continue to offer doctors and their patients technologically advanced and high quality medical devices and therapies.

Device Description

The ENDOTAK RELIANCE® G lead, Models 0184/0185/0186/0187, and the ENDOTAK RELIANCE® SG lead, Models 0180/0181/0182/0183, are endocardial cardioversion/defibrillation, pace/sense, steroid-eluting, and active fixation leads with an extendable/retractable helix. The silicone lead body has a lubricious coating. The electrode coils are covered with GORE® expanded polytetrafluoroethylene (ePTFE). The ENDOTAK RELIANCE (dual-coil leads) and the ENDOTAK RELIANCE SG (single-coil leads) are for use as an integral part of an ICD automatic implantable cardioverter defibrillator system with DF-1¹ and IS-1² ports.

Instructions in this manual should be used in conjunction with other resource material, including the applicable ICD physician's manual and instructions for use on any implant accessories or tools.

Indications for Use

The ENDOTAK RELIANCE lead, Models 0184/0185/0186/0187, and the ENDOTAK RELIANCE SG lead, Models 0180/0181/0182/0183, provide pacing and rate-sensing and deliver cardioversion and defibrillation shocks for ICD automatic implantable cardioverter defibrillator systems.

Contraindications

Use of the ENDOTAK RELIANCE G and ENDOTAK RELIANCE SG active fixation lead is contraindicated for the following patients:

- Patients who have a unipolar pacemaker.
- Patients with a hypersensitivity to a nominal single dose of 1.0 mg dexamethasone acetate.
- Patients with mechanical tricuspid heart valves.

Warnings

In the following list of warnings, page numbers are indicated for those warnings that are specific to other areas of the manual. Refer to the indicated pages for information relevant to the warning.

1. DF-1 refers to the international standard ISO 11318:2002.
2. IS-1 refers to the international standard ISO 5841.3:2000.

GORE is a trademark of W. L. Gore and Associates.

ICD/Lead Compatibility

- Do not attempt to use the ENDOTAK lead system with any device other than a commercially available implantable defibrillator system with which it has been tested and demonstrated to be safe and effective. The potential adverse consequences of using a combination that has not been tested and demonstrated to be safe and effective may include, but are not limited to, undersensing cardiac activity and failure to deliver necessary therapy.

MRI Exposure

- Do not expose a patient to the MRI environment. Strong electromagnetic fields in the MRI environment may interfere with the pulse generator and lead system and cause injury to the patient.

Diathermy Exposure

- Do not expose a patient to diathermy treatment. Shortwave or microwave diathermy may cause injury to the patient.

Implantation

- The safety and efficacy of the tip electrode placement above midseptum has not been clinically established.
- Lead fracture, dislodgment, abrasion and/or an incomplete connection can cause a periodic or continual loss of rate-sensing, possibly resulting in arrhythmia nondetection; or over-sensing of rate, possibly resulting in inappropriate delivery of a pulse generator shock; or inadequate delivery of converting energy.
- Although pliable, the lead is not designed to tolerate excessive flexing, bending, or tension. This could cause structural weakness, conductor discontinuity, and/or lead dislodgment. (Page 14)
- Take care to obtain appropriate electrode position. Failure to do so may result in higher defibrillation thresholds or may render the lead unable to defibrillate a patient whose tachyarrhythmia(s) might otherwise be convertible by an ICD system. (Page 19)
- In order to deliver defibrillation therapy, the single-coil ENDOTAK RELIANCE SG lead must be implanted with a separate defibrillation electrode. Boston Scientific recommends using the ENDOTAK RELIANCE SG lead with a pectorally implanted device that uses the metallic housing as a defibrillation electrode. (Page 19)

Electrical Performance

- When connecting the lead to the ICD pulse generator, it is very important that proper connections are made. Damage to the heart could

result if a high-voltage defibrillating pulse were to be delivered through the pace/sense tip electrode. (Page 23)

Conversion Testing

- Use of any component of the ENDOTAK lead system to assist in delivery of external-source rescue shocks could cause extensive tissue damage. (Page 24)

Securing and Tunneling

- Do not kink, twist, or braid the lead terminals as doing so could cause lead insulation abrasion damage. (Page 27)

Single Use Only

- For single patient use only. Do not reuse, reprocess, or resterilize. Reuse, reprocessing, or resterilization may compromise the structural integrity of the device and/or lead to device failure which, in turn, may result in patient injury, illness, or death. Reuse, reprocessing, or resterilization may also create a risk of contamination of the device and/or cause patient infection or cross-infection, including, but not limited to, the transmission of infectious disease(s) from one patient to another. Contamination of the device may lead to injury, illness, or death of the patient.

Precautions

- Tricuspid valvular disease may be exacerbated by the presence of a lead. Use medical judgment when deciding to place a lead in a patient with tricuspid valvular disease.
- It has not been determined whether the warnings, precautions, or complications usually associated with injectable dexamethasone acetate apply to the use of the low concentration, highly localized, controlled-release device. Refer to the Physicians' Desk Reference® for a listing of potentially adverse effects.
- Refer to the Implant Information, Implantation and Post-implant Evaluation sections of this manual for cautions specific to handling, implanting, and testing the ENDOTAK RELIANCE lead family. Failure to observe these cautions could result in incorrect lead implantation, lead damage, and/or harm to the patient.

Adverse Events

Given the similar design features, including the active fixation helix and steroid elution, the ENDOTAK RELIANCE/S (models 0137-0139, 0153, and 0157-0159) clinical investigation was used to support the active-fixation ENDOTAK RELIANCE G/SG models 0180-0187. The following are the adverse events reported in that investigational study.

Observed Adverse Events

A confirmatory clinical investigation was conducted on the ENDOTAK RELIANCE lead, Models 0157/0158/0159. The complications and observations are reported in Table 1.

Table 1. ENDOTAK RELIANCE Lead, Ventricular Morbidity^a

	# of pts. ^b (n = 30)	% of pts. (95% CI)	# of Leads	Adverse Events per Lead-Month
Complications^c (total)	0	-	0	0%
Observations^d (total)	0	-	0	0%

a. Adverse event data is derived from 30 patients followed for 30 days.

b. Patients and leads may have multiple adverse events.

c. Complications are defined as adverse events requiring invasive measures to correct (eg, surgical intervention).

d. Observations are defined as adverse events which are correctable by noninvasive measures (eg, reprogramming).

Potential Adverse Events

Based on the literature and lead implant experience, the possible physical effects from implantation of an ENDOTAK RELIANCE lead are listed below in alphabetical order:

- Air embolism
- Allergic reaction
- Bleeding
- Cardiac perforation/tamponade
- Chronic nerve damage
- Component failures
- Conductor coil fracture
- Death
- Erosion/extrusion
- Excessive fibrotic tissue growth
- Extracardiac stimulation (muscle/nerve stimulation)
- Formation of hematomas or cysts
- Inability to provide therapy
- Inappropriate therapy/shocks
- Incomplete connection with pulse generator
- Infection
- Keloid formation
- Lead abrasion
- Lead displacement/dislodgment
- Lead fracture, insulation break
- Lead tip deformation and/or breakage
- Local tissue reaction
- Low amplitude VF signals
- Myocardial injury
- Myocardial irritability
- Myopotential sensing
- Oversensing/undersensing
- Pericardial rub, effusion
- Pneumothorax
- Post-shock rhythm disturbances
- Shunting current or insulating myocardium during defibrillation with internal or external paddles
- Tachyarrhythmias, which include acceleration of arrhythmias and early, recurrent atrial fibrillation
- Threshold elevation
- Thrombosis/thromboemboli
- Valve damage
- Venous occlusion
- Venous perforation/erosion

Clinical Investigations

Two clinical studies were used to support this lead. The first study involving the ENDOTAK RELIANCE lead, models 0157/0158/0159, examined electrical performance and confirmed clinical acceptability of the ventricular voltage threshold, the ventricular lead pacing impedance and the R-wave sensing. The second study, the ENDOTAK RELIANCE G, models 0164/0165/0167, lead study, examined defibrillation performance (DFT) of a lead with ePTFE (Gore) covered shocking coils.

Electrical Performance

The confirmatory clinical investigation was an evaluation of the ENDOTAK RELIANCE lead, Models 0157/0158/0159 in 30 patients. The confirmatory clinical investigation provided reasonable assurance of the safety and effectiveness of the ENDOTAK RELIANCE lead system. Lead safety was supported by a review of lead-related complications. In 30 implanted leads, there were no lead-related complications. Patient population characteristics and electrical performance are summarized in the tables below.

Table 2. Patient Population Characteristics (N = 30 patients)

Category	ENDOTAK RELIANCE lead, Models 0157/0158/0159
Number of Patients Attempted (N)	0
Number of Patients Implanted (N)	30
Age at Implant (years)	
N	30
Minimum	55.7
Maximum	86.5
Mean	68.5
Standard Deviation	9.1
Gender	
Male	23 (76.7%)
Female	7 (23.3%)
Left Ventricular Ejection Fraction (LVEF) (%)	
N	30
Minimum	15.0
Maximum	55.0
Mean	29.4

Table 3. Mean Ventricular Voltage Threshold at 0.5 ms by Follow-up Period (N = 30 patients)

Follow-up	ENDOTAK RELIANCE lead, Models 0157/0158/0159		
	Number of Patients	Mean (V)	Standard Deviation
Pre-discharge	29	0.5	0.2
1 month	29	0.8	0.3

Table 4. Ventricular Lead Pacing Impedance by Follow-up Period

Follow-up	ENDOTAK RELIANCE lead, Models 0157/0158/0159		
	Number of Patients	Mean (Ω)	Standard Deviation
Pre-discharge	30	568	98.2
1 month	29	530	66.2

Table 5. R-wave Sensing Amplitudes by Follow-up Period

Follow-up	ENDOTAK RELIANCE lead, Models 0157/0158/0159		
	Number of Patients	Mean (mV)	Standard Deviation
Pre-discharge	30	14.3	5.9
1 month	29	16.2	6.4

DFT Performance

Clinical data from the ENDOTAK RELIANCE G lead study, models 0164/0165/0167, are used to support DFT performance of a lead with Gore covered shocking coils.

The RELIANCE G study was a prospective, multi-center (17 centers), US clinical evaluation utilizing the ENDOTAK ENDURANCE EZ® leads (referred to as the ENDURANCE EZ leads) as a historical control. Ninety-five patients were enrolled in the study from August 15, 2002 through November 21, 2002. A total of 85 patients (70 male, 15 female) were successfully implanted with the RELIANCE G lead (models 0164/0165/0167), one was attempted, and 9 were intents.

The DFT at implant met the recommended acceptable implant criteria of < 21 J as defined in the physician's manual.

A total of 39 patients received step-down DFT testing at implant. Table 6 lists the mean DFT for these patients.

Table 6. ENDOTAK RELIANCE G DFT Testing at Implant

Device	N	Mean	Standard Deviation	Min	Max
ICD and Lead Alone	39	9.2	4.5	3	17

The mean DFT value for the RELIANCE G lead was 9.2, which is similar to the mean DFT value of 9.3 for the historical control lead (ENDURANCE EZ).

Warranty

See the enclosed Lead Information card for warranty information. For additional copies, please contact Boston Scientific at the address on the back cover.

Refer to the Contraindications, Warnings, Precautions, and Adverse Events sections of this manual for information concerning the performance of this device.

Lead Features

Features of the ENDOTAK RELIANCE G and ENDOTAK RELIANCE SG active fixation lead include the following components:

- **Steroid Distal Tip:** The tip electrode contains a nominal dose of 1.0 mg dexamethasone acetate within a silicone collar. Upon exposure to body fluids, the steroid elutes from the external collar. Steroid suppresses the inflammatory response believed to cause threshold rises typically associated with implanted pacing electrodes. Lower thresholds are desirable because they can increase pacing safety margins and reduce pacing energy requirements, potentially increasing pulse generator longevity.
- **Extendable/Retractable Fixation Helix:** The extendable/ retractable helix design anchors the distal tip electrode to the endocardial surface without support of trabecular structures, offering various lead placement possibilities for the tip electrode. The extendable/retractable helix serves as the cathode for intracardiac right ventricular electrogram rate sensing and pacing. The helix is extended/retracted using a terminal pin mechanism.
- **Fluoroscopic Markers:** The lead has radiopaque markers near the distal tip that can be seen under fluoroscopy. These markers show when the helix is fully retracted or fully extended.
- **Coil Electrodes:** The distal coil electrode is intended to serve as an anode for rate-sensing and pacing and as an anode or cathode for cardioversion/defibrillation shocks. The proximal coil electrode on the ENDOTAK RELIANCE lead is intended to serve as an anode or cathode for cardioversion/defibrillation shocks. The ENDOTAK RELIANCE lead family uses the implanted device metallic housing as an additional defibrillation electrode.
- **GORE ePTFE-Covered Coils:** The ePTFE covering over the defibrillation coils prevents tissue ingrowth around and between the coil filars.

- **Lead Body:** The isodiametric lead body contains one conductor for pacing/sensing. The ENDOTAK RELIANCE lead has two conductors for defibrillation and the ENDOTAK RELIANCE SG lead has one conductor for defibrillation. The conductors are coated with PTFE and insulated in separate lumens within the silicone rubber lead body. A second layer of silicone covers the lead body, providing additional insulation and a uniform body diameter. The terminal yoke, suture sleeves, and terminal moldings are fabricated from molded silicone rubber. A color-coded mark on the terminal end of the lead allows for a quick visual reference of the lead length. The lead color matches the same length stylet cap color.
- **Lubricious Coating:** The ENDOTAK RELIANCE lead family is the first to introduce a proprietary coating that makes the silicone lead surface more lubricious. The lubricious coating reduces both the static and dynamic coefficients of friction, making the lead surface feel and handle like polyurethane while providing the time-tested reliability of silicone.
- **Terminals:** The ENDOTAK RELIANCE lead has three terminals: two DF-1 (shock), and one bipolar IS-1 (pace/sense). The ENDOTAK RELIANCE SG lead has two terminals: one DF-1 (shock), and one bipolar IS-1 (pace/sense). The pace/sense terminal is tubular and is fitted with a stylet guide to facilitate the insertion of a stylet.

The lead is intended for chronic implantation within the superior vena cava, right atrium, and right ventricle. The extendable/retractable helix design provides various lead placement possibilities for the tip electrode in the right ventricle. Refer to Figure 11 and Figure 12 for suggested lead positioning. When connected to the ICD pulse generator, the implanted lead will perform the following functions:

- Provide rate-sensing and shocking electrode electrograms
- Deliver cardioverting/defibrillating electrical shocks from the pulse generator to the heart
- Provide pacing capabilities

Nominal overall lengths of the active fixation leads are as follows:

ENDOTAK RELIANCE G	0184	0185	0186	0187
	59 cm	64 cm	70 cm	90 cm
ENDOTAK RELIANCE SG	0180	0181	0182	0183
	59 cm	64 cm	70 cm	90 cm

The nominal electrode spacing (measured from the distal tip base to the distal end of the proximal coil electrode) of the ENDOTAK RELIANCE lead is 18 cm (Figure 1).

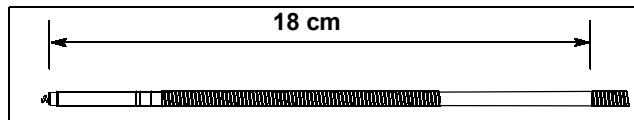


Figure 1. Electrode spacing for the ENDOTAK RELIANCE lead is measured from the distal tip base to the distal end of the proximal coil electrode.

Lead Evaluation

Implant Information

Proper surgical procedures and techniques are the responsibility of the medical professional. The described implant procedures are furnished only for informational purposes. Each physician must apply the information in these instructions according to professional medical training and experience.

A major consideration in choosing the ENDOTAK RELIANCE lead family is that it does not require a thoracotomy. The physician should weigh its advantages against the patient's ability to withstand additional electrophysiology (EP) testing (arrhythmia induction and conversion testing)—and a possible thoracotomy—should the lead system prove ineffective.

Various factors, such as cardiomegaly or drug therapy, may necessitate repositioning of the defibrillation leads or substitution of one lead system for another in order to facilitate arrhythmia conversion. **In some cases, reliable arrhythmia conversion may not be obtained with any leads at the available ICD energy levels.**

Bipolar pacemakers may be used with the ENDOTAK RELIANCE lead family and ICD pulse generator as long as the pacemaker and ICD pulse generator do not interact, causing ICD pulse generator nondetection or false detection. Refer to the section, Minimizing Pacemaker Interaction on Page 22 for more information.

The lead is not designed, sold, or intended for use except as indicated.

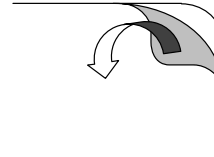
The following items are packaged with the ENDOTAK RELIANCE G and ENDOTAK RELIANCE SG active fixation lead:

- Straight stylets, soft^a
- Straight stylets, firm^b
- Fixation tools
- Stylet guide

- Transvalvular Insertion (TVI) tool
 - Vein pick
 - Lead caps, (2) DF-1 and (1) IS-1
 - DF-1 port plugs (ENDOTAK RELIANCE SG lead only)
 - Literature packet
- a. Green knobs, 0.014-in (0.36-mm) diameter
 - b. White knobs, 0.016-in (0.41-mm) diameter

Opening Instructions

The outer package and sterile tray may be opened by authorized personnel under clean conditions. To ensure sterility, the sealed inner sterile tray must be opened using accepted aseptic technique by scrubbed, masked, sterile-gowned personnel. The sterile tray is opened by peeling back the cover.



Sterilization

Boston Scientific sterilizes the lead and accessories with ethylene oxide gas (EO) before final packaging. When they are received, they are sterile and ready for use. If the container is wet, damaged, punctured, or if the seal is broken, return the lead to the nearest Boston Scientific representative. Never attempt to resterilize the lead.

Storage

Recommended storage temperature range is 0°C to 50°C.

Surgical Preparation

Instrumentation for cardiac monitoring, imaging (fluoroscopy), defibrillation, and lead signal measurements must be available during implant. When using electrical instrumentation, electrically isolate the patient from potentially hazardous current leakage. Boston Scientific also recommends availability of sterile duplicates of all implantable items in case of accidental damage or contamination.

Accessories

Suture Sleeves

Suture sleeves are an adjustable, tubular reinforcement positioned over the outer lead insulation (Figure 2). They are designed to secure and protect the lead after distal electrode fixation. Using suture sleeves optimizes lead longevity and reduces the possibility of structural damage caused by suturing directly over the lead body.

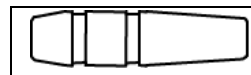


Figure 2. The long tapered end of the suture sleeve faces toward the vein.

To move a suture sleeve, gently twist and pull it over the lead until it is in the desired position.

CAUTION: Do not suture directly over the lead body, as this may cause structural damage. Use the suture sleeves to secure the lead lateral to the venous entry site.

The following items are packaged with the lead and are also available from Boston Scientific as accessory items:

Fixation Tool

The fixation tool can be attached to the terminal pin and rotated clockwise or counterclockwise for extending or retracting the helix (Figure 3).

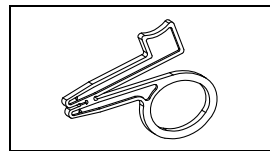


Figure 3. The fixation tool.

Stylets

Firm and soft positioning stylets are packaged with each lead. A stylet inserted in the lead aids in positioning the lead tip in the heart. The stylet length is imprinted on the color-coded cap of the knob (Table 7). Also refer to “Inserting the Stylet” (Page 15), for more information.

Table 7. Stylets

	Stylet Length (cm)	Knob Color	Cap Color
Straight	59	Green = Soft or White = Firm	Yellow
	64		Green
	70		Black
	90		Orange

Stylet Guide

A stylet guide is packaged with the lead and is intended to ease insertion of a stylet into the pace/sense terminal of the lead (Figure 4).

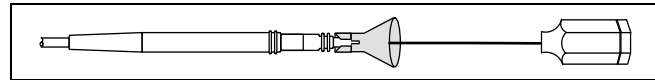


Figure 4. Using the stylet guide.

Transvalvular Insertion Tool

The Transvalvular Insertion (TVI) tool is a sterile, disposable, nontoxic, plastic device designed to allow the use of tear-away hemostatic introducers with the ENDOTAK RELIANCE G and ENDOTAK RELIANCE SG lead families. The TVI tool is used to temporarily dilate the hemostatic valve thereby allowing the e-PTFE-covered coils to freely pass through the hemostatic valve (Figure 5).

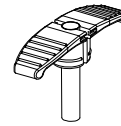


Figure 5.
TVI tool.

The following are techniques that may be used for the implant procedure with the TVI tool:

1. Step 1 may vary depending on whether or not a guide wire is used to place the lead. It is recommended that step 1B be used when retaining a guide wire.
 - A.** Following insertion of the hemostatic introducer into the vein and removal of the dilator, insert the distal tip of the lead into the TVI tool such that the distal tip is flush or slightly recessed from the distal end of the TVI tool. Grasp the lead and TVI tool combination with your thumb and first finger and insert the assembly into the proximal end of the hemostatic introducer by gently pushing the lead and TVI tool through the hemostatic valve. The TVI tool is fully inserted when the base of its handle contacts the proximal end of the introducer.
 - B.** Following insertion of the hemostatic introducer into the vein and removal of the dilator, hold your thumb over the proximal exposed opening of the TVI tool and insert the distal end of the TVI tool into the proximal end of the hemostatic introducer by gently pushing the TVI tool through the hemostatic valve.

Note: *When retaining a guide wire, the TVI tool must be placed over the guide wire and not along the side of it.*

Continue to hold your thumb over the proximal exposed opening of the TVI tool to prevent air embolization and/or back bleeding. The TVI tool is fully inserted when the base of its handle contacts the proximal end of the introducer.

2. Advance the lead through the TVI tool and into the introducer. Continue to advance the lead until the shocking coil(s) is past the hemostatic valve.
3. When the lead is resting inside the introducer, pull the TVI tool out of the hemostatic valve. The TVI tool may be temporarily left on the body of the lead to facilitate repositioning. Once the lead is in position, the TVI tool must be peeled away.

Vein Pick

The vein pick is a sterile, disposable, nontoxic, nonpyrogenic, plastic device designed to assist the physician during entry of the lead's electrode tip into the vein.

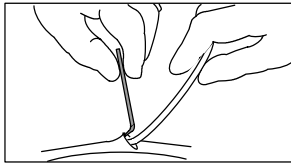


Figure 6. Using the vein pick.

To use the vein pick during a cutdown procedure, isolate and open the selected vein using an appropriate scalpel or scissors. Introduce the point of the vein pick via this incision into the lumen of the vein (Figure 6). With the point of the vein pick facing in the direction of the desired lead passage, gently raise and tilt the pick. Pass the lead under the vein pick and into

the vein.

CAUTION: The vein pick is not intended either for puncturing the vein or for dissecting tissue during a cutdown procedure. Be sure that the vein pick does not puncture the silicone rubber insulation of the lead. This could prevent proper lead function.

Lead Caps

The silicone rubber lead caps should be used to protect the lead terminals during the procedure. Lead caps may also be used to isolate or cap any lead terminal not inserted into the ICD pulse generator. Placing a suture in the lead cap groove will secure the lead cap to the lead terminal.

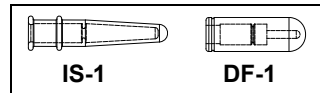


Figure 7. Use IS-1 lead caps on IS-1 terminals and DF-1 lead caps on DF-1 terminals.

Handling the Lead

Observe the following when handling the lead:

WARNING: Although pliable, the lead is not designed to tolerate excessive flexing, bending, or tension. This could cause structural weakness, conductor discontinuity, and/or lead dislodgment.

CAUTIONS:

- Avoid holding or handling the distal tip of the lead.
- **Do not wipe or immerse the electrode in fluid.** Such treatment will reduce the amount of steroid available when the lead is implanted.
- Chronic repositioning may adversely affect the lead's low-threshold performance because the steroid may be depleted.

- Do not attempt to alter the electrodes. Do not apply pressure to the tip of the electrode.
- The conductor insulation is silicone rubber, which can attract particulate matter and must always be protected from surface contamination.
- Do not apply oil-based lubricants to the ePTFE-covered shocking coils.

Note: *Boston Scientific suggests using sterile water if a lubricant is needed when coupling the lead with the ICD pulse generator.*

Implantation

Inserting the Stylet

Choose a stylet according to the function and to the firmness desired. Remove the preinserted stylet before inserting a different one. Make sure the stylet is fully inserted in the lead prior to inserting the lead into the vein.

Gently curve the preferred straight stylet with any sterile, smooth-surfaced instrument (eg, 10- or 12-cc syringe barrel) (Figure 8) and carefully insert the stylet through the lumen of the conductor. A sharp bend in the stylet may straighten as it passes through the lumen of the terminal pin. A gentle curve is less likely to straighten.

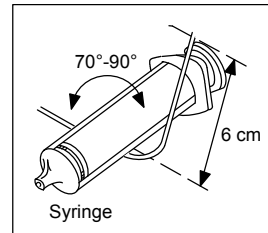


Figure 8. Curve the stylet.

CAUTION: Do not bend the lead with a stylet in place. Bending the lead could damage the conductor and insulation material.

Note: *To optimize insertion into the lead, do not allow body fluids to come in contact with the stylet.*

Handling the Fixation Helix

Before implanting the lead, verify the mechanical functioning of the lead by rotating the terminal pin and visually observing the helix extending and retracting. The helix can be extended or retracted by rotating the terminal pin clockwise to extend the helix or counterclockwise to retract it.

Note: *Refer to the Lead Fixation section on Page 20 for additional information on how to fixate the helix and to the Specifications section on Page 31 for the expected and maximum number of turns to extend or retract the helix.*

CAUTIONS:

- Do not overextend or overretract the helix. Continuing to rotate the terminal pin once the helix is fully extended or retracted can damage the lead.
- If the helix cannot be extended or retracted, do not use the lead.
- Do not alter the electrodes or use a lead with a deformed helix or damaged helix fixation mechanism. **Do not attempt to straighten or realign the fixation helix.**

Notes:

- *Do not insert a lead into the vein when the helix is extended. Rotate the terminal pin counterclockwise to retract the helix into the distal lead tip prior to insertion into the vein.*
- *Any curves introduced into the stylet could increase the number of turns needed to extend or retract the helix.*

Inserting the Lead

The lead may be inserted using one of the following methods:

- Via cutdown through the left or right cephalic vein.

Only one incision (below the clavicle) is required to insert the lead through the cephalic vein. The endocardial lead is inserted into the right or left cephalic vein in the deltopectoral groove.

The vein pick packaged with this lead can be used during a cutdown procedure to aid insertion of the lead into the vein. Before inserting the lead, refer to the Accessories section for instructions on using the vein pick.
- Percutaneously or via cutdown through the subclavian vein or internal jugular vein-typically the left subclavian or right internal jugular vein.
 - A 9F subclavian introducer set is available from Boston Scientific for use during percutaneous lead insertion.
 - When using a hemostatic tear-away introducer, use the TVI tool packaged with this lead. The recommended hemostatic tear-away introducer size is 9.5F (3.17 mm). Refer to the Accessories section for detailed instructions for use.

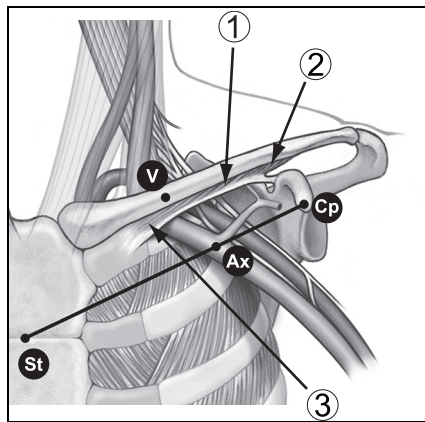
CAUTIONS:

- The TVI tool should always be used in conjunction with a hemostatic tear-away introducer.
- When attempting to implant the lead via a subclavian puncture, do not insert the lead under the medial one-third region of the clavicle. Damage

to the lead is possible if the lead is implanted in this manner. If implantation via the subclavian vein is desired, the lead must enter the subclavian vein near the lateral border of the first rib and must avoid penetrating the subclavius muscle. It is important to observe these implant precautions in order to avoid clavicle/first rib damage to the lead. It has been established in the literature that lead fracture can be caused by lead entrapment in such soft tissue structures as the subclavius muscle, costocoracoid ligament, or the costoclavicular ligament.³

Leads placed by percutaneous subclavian venipuncture should enter the subclavian vein where it passes over the first rib (rather than more medially) to avoid entrapment by the subclavius muscle or ligamentous structures associated with the narrow costoclavicular region.⁴ Boston Scientific recommends introducing the lead into the subclavian vein near the lateral border of the first rib.

The syringe should be positioned directly above and parallel to the axillary vein to reduce the chance that the needle will contact the axillary or subclavian arteries or the brachial plexus. Use of fluoroscopy is helpful in locating the first rib and in guiding the needle. The steps below explain how to identify the skin entry point and define the course of the needle toward the subclavian vein where it crosses the first rib.



- [1] Subclavius muscle
- [2] Costocoracoid ligament
- [3] Costoclavicular ligament

Figure 9 Landmarks identify the entry point for a percutaneous subclavian venipuncture.

1. Referring to Figure 9, identify points St (sternal angle) and Cp (coracoid process).

3. Magney JE, et al. Anatomical mechanisms explaining damage to pacemaker leads, defibrillator leads, and failure of central venous catheters adjacent to the sternoclavicular joint. PACE. 1993; 16:445-457.
4. Magney JE, et al. A new approach to percutaneous subclavian venipuncture to avoid lead fracture or central venous catheter occlusion. PACE. 1993;16:2133-2141.

2. Visually draw a line between St and Cp, and divide the segment into thirds. The needle should pierce the skin at the junction of the middle and lateral thirds, directly above the axillary vein (point Ax).
3. Place an index finger on the clavicle at the junction of the medial and middle thirds (point V), beneath which point the subclavian vein should be located.
4. Press a thumb against the index finger and project one or two centimeters below the clavicle to shield the subclavius muscle from the needle (when hypertrophy of the pectoralis muscle is apparent, the thumb should project about two centimeters below the clavicle because the subclavius muscle should be hypertrophied as well) (Figure 10).
5. Feel with the thumb the pressure from the passage of the needle through the superficial fascia; direct the needle deep into the tissues toward the subclavian vein and the underlying first rib. Fluoroscopic guidance will reduce the chance that the needle would pass below the first rib and into the lung.

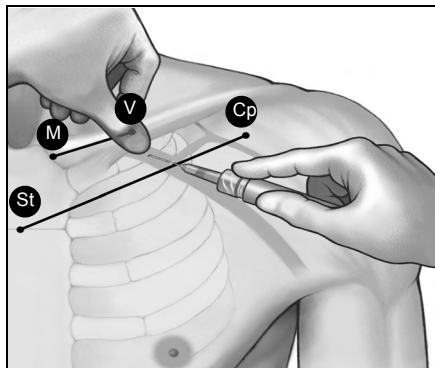


Figure 10. Location of thumb and needle entry.

Positioning the Lead

Under fluoroscopy and with the helix retracted and a stylet in the lead, advance the lead as far as possible so the tip electrode is in the apex of the right ventricle (Figure 11 and Figure 12). Also verify under fluoroscopy that the distal coil electrode is situated in the right ventricle, below the tricuspid valve, and that the proximal coil electrode (ENDOTAK RELIANCE lead models only) is situated in the superior vena cava and high right atrium. **Correct functioning of the lead depends on appropriate placement of the electrodes.**

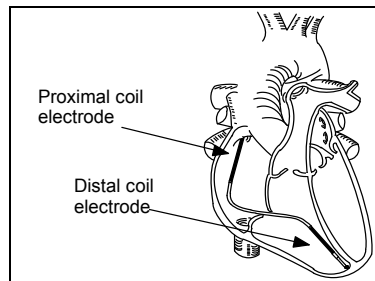


Figure 11. Suggested electrode position within the heart for ENDOTAK RELIANCE leads.

Notes: *When the lead is used with an ICD with pacing capability, position the distal tip in healthy myocardium in the apex of the heart.*

WARNINGS:

- Use fluoroscopy to verify that the lead tip is directed toward the apex when implanted. Other positions may result in lead movement which could affect defibrillation efficacy.
- Take care to obtain appropriate electrode position. Failure to do so may result in higher defibrillation thresholds or may render the lead unable to defibrillate a patient whose tachyarrhythmia(s) might otherwise be convertible by an ICD system.
- In order to deliver defibrillation therapy, the single-coil ENDOTAK RELIANCE SG lead must be implanted with a separate defibrillation electrode. Boston Scientific recommends using the ENDOTAK RELIANCE SG lead with a pectorally implanted device that uses the metallic housing as a defibrillation electrode.

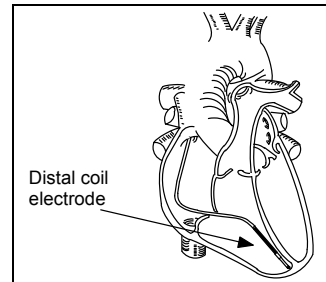


Figure 12. Suggested electrode position within the heart for ENDOTAK RELIANCE SG leads.

CAUTION: For patients with bipolar cardiac pacemakers, the lead pace/sense electrode (the tip electrode and distal coil electrode) should be placed as far as possible from the pacemaker electrodes to avoid cross-sensing between the ICD and the pacemaker.

Lead Fixation

The ENDOTAK RELIANCE G and ENDOTAK RELIANCE SG active fixation lead's helix is electrically conductive to allow mapping of potential electrode positions. Mapping means pacing and sensing thresholds can be measured without extending the helix into the tissue. Rather, the distal tip of the lead can be placed against the tissue and measurements can be taken. If data is acceptable, proceed with lead fixation. Mapping of the ventricle prior to lead fixation is recommended as it can reduce the potential need for multiple lead positionings.

Note: *The stylet must be fully inserted during fixation or repositioning.*

1. When the correct position has been achieved, attach the fixation tool to the terminal pin. Press the handles together and place the pin in the preformed groove. Release the tension on the handles to secure the terminal pin in the fixation tool (Figure 13).

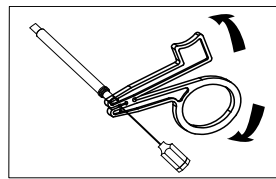


Figure 13. Attaching and rotating the fixation tool.

2. Apply forward pressure to the lead body to position the distal electrode against the desired fixation site and rotate the fixation tool *clockwise* to affix the distal electrode helix into the heart wall. View the radiopaque markers under fluoroscopy to identify when the fixation helix is fully extended. Full extension is achieved when the radiopaque markers are joined and the fixation helix is extended outside the distal fluoroscopy markers (Figure 14). Refer to the Specifications section on Page 31 for the expected number of turns to extend or retract the helix.

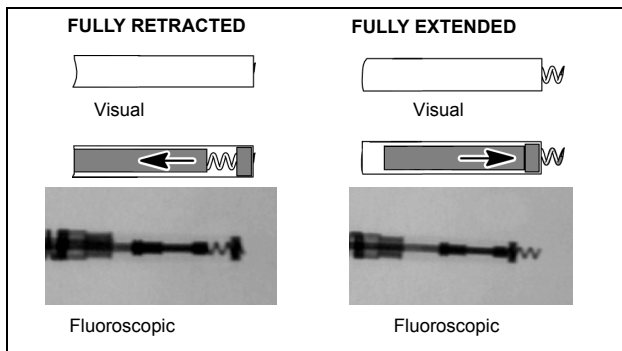


Figure 14. Possible views of the helix electrode.

CAUTION: Do not rotate the terminal pin clockwise more than the maximum number of turns indicated for each model number in the

Specifications section on Page 31. Continuing to rotate the terminal pin once the helix is fully extended or retracted (as indicated by fluoroscopy) can damage the lead, cause lead dislodgment, and/or cause acute pacing threshold to rise.

Note: *Stylet curvature, extended implant time, and repositioning the lead multiple times may increase the number of turns to extend or retract the helix.*

3. Loosely hold the proximal end of the lead and release the fixation tool.

Note: *After Step 3, minimal counterrotation in the terminal pin may be observed.*

4. Remove the fixation tool from the terminal pin by pressing the handles of the tool together.

If the helix mechanism fails to function properly during repositioning, the following caution must be carefully observed to avoid possible tissue snagging when removing the lead:

CAUTION: Do not use the lead if the helix cannot be retracted during implant. Continuous *counterclockwise* rotation of the lead body during lead removal is necessary to avoid inadvertent tissue trauma. Counterclockwise lead rotation helps to prevent accidental fixation and releases the electrode helix if tissue snagging has occurred.

Checking for Lead Stability

After fixation, partially withdraw the stylet 8 to 10 cm. Check the stability of the lead using fluoroscopy. If possible, have the patient cough or take several deep breaths. When electrode position is satisfactory, completely withdraw the stylet.

CAUTION: Should dislodgment occur, immediate medical care is required to resolve the electrode position and minimize endocardial trauma.

Repositioning the Lead

If the lead needs repositioning, verify the stylet is fully inserted in the lead, reconnect the fixation tool, and rotate the tool *counterclockwise* to retract the helix. Use fluoroscopy to verify that the helix is retracted and disengaged completely from the heart wall before attempting to reposition the lead. Reaffix the electrode (helix) using the procedures previously discussed in the Positioning the Lead, Lead Fixation, and Checking for Lead Stability sections. Do not rotate the fixation tool more than the maximum number of turns indicated in the Specifications (Page 31). Continuing to rotate the terminal pin once the helix is fully extended or retracted (as indicated by fluoroscopy) can damage the lead.

Evaluating Lead Position

Verify electrical performance of the lead *before* attaching the lead to the pulse generator and *after* allowing sufficient time for the effect of local tissue trauma to subside. The use of radiography or fluoroscopy during the operation may help ensure lead position and integrity. If testing results are unsatisfactory, lead system repositioning or replacement may be required.

Minimizing Pacemaker Interaction

To minimize potential interaction between a permanent pacemaker and an ICD pulse generator, consider the following:^{5 6}

- After implanting the pacing leads, examine the signals from the pace/sense electrodes to ensure that minimal pacemaker artifacts are present. (Use a recording system that has a bandwidth of at least 2000 Hz to ensure that minimal pacemaker artifacts are present.)
- All of the patient's ventricular tachyarrhythmias and ventricular fibrillation should be induced while the ICD pulse generator is activated and the pacemaker is programmed to an asynchronous mode at maximum output. This should provide the greatest opportunity for inhibition of arrhythmia detection due to pacemaker artifacts. The pacing leads may have to be repositioned to eliminate artifacts.
- Since it is difficult to predict the relative magnitudes of pacemaker artifacts and various tachyarrhythmia electrograms that may occur chronically or during EP testing, it is important to reduce artifacts to the minimum.
- Consider programming the pacemaker to (1) the lowest amplitude allowable for safe capture in the chronic state, (2) the maximum sensitivity, and (3) the minimum cardiac rate acceptable for the patient. Also consider using pacemaker leads with close interelectrode spacing (eg, 1–2 cm).

Taking Baseline Measurements

Connect the terminal pins to a pacing system analyzer (PSA) and evaluate the placement by determining the following:

- R-wave amplitude
- Pacing threshold
- Pacing lead impedance

Note that the pulse generator measurements may not exactly correlate to the PSA measurements due to signal filtering. Baseline measurements should fall within the recommended values listed in Table 8.

5. Epstein AE, et al. Combined automatic implantable cardioverter-defibrillator and pacemaker systems: implantation techniques and follow-up. *JACC*. 1989;13:121-131.
6. Calkins H, et al. Clinical interactions between pacemakers and automatic implantable cardioverter-defibrillators. *JACC*. 1990;16:666-673.

Table 8. Recommended Lead Signal Parameters^a

Signal Type	Amplitude a, b, c	Duration a, b, c	Pacing Threshold ^d	Impedance
Pacing/ Sensing	≥5 mV	<100 ms	≤1.5 V	300–1200 Ω
Defibrillation	≥1 mV	<150 ms	NA	20–125 Ω

- a. Measured approximately 10 minutes after placement.
b. This measurement is not inclusive of current injury.
c. In normal sinus rhythm.
d. Pulse width setting at 0.5 ms.

Lower intrinsic potentials, longer durations, and higher pacing thresholds may indicate lead placement in ischemic or scarred tissue. Because signal quality may deteriorate, reposition the lead if necessary to obtain a signal with the largest possible amplitude, shortest duration, and lowest pacing threshold.

Changes in the defibrillation electrode surface area, such as changing from a TRIAD configuration to a single coil configuration, can affect the impedance measurements. Baseline defibrillation impedance measurements should fall within the recommended values indicated in the table.

CAUTION: R-wave amplitudes of less than the recommended value can cause inaccurate rate counting in the chronic state, possibly resulting in failure to sense a tachyarrhythmia or misdiagnosis of a normal rhythm as abnormal. Signal durations that exceed the programmed refractory period of the ICD pulse generator can cause inaccurate cardiac rate determination or inappropriate high-voltage shock delivery or both.

If the measurements do not conform to these values, reinsert the stylet and reposition the lead using the procedures previously discussed. Verify that measurements fall within the recommended values. If testing results are unsatisfactory, further lead system repositioning or replacement may be required.

Electrical Performance

Make the lead connections and evaluate the lead signals using the pulse generator.

WARNING: When connecting the lead to the ICD pulse generator, it is very important that proper connections are made. **Damage to the heart could**

result if a high-voltage defibrillating pulse were to be delivered through the pace/sense tip electrode.

Evaluating with the Pulse Generator

Connect the terminal pins to the pulse generator and place the ICD pulse generator into the ICD implant pocket as indicated in the ICD physician's manual. Also, refer to "Connection to a Pulse Generator" (Page 28) for more information.

Evaluate the lead signals by viewing the real-time EGM. The signal from the implanted lead should be continuous and without artifact, similar to a body-surface ECG. A discontinuous signal may indicate a lead fracture or an otherwise damaged lead, or an insulation break that would necessitate lead replacement. Inadequate signals may result either in a failure of the ICD system to detect an arrhythmia or in an unnecessary delivery of therapy.

Evaluating with the PRM

Evaluate the lead signals using the Programmer/Recorder/Monitor (PRM) programming system or an external strip chart recorder. As seen on the strip chart recorder, the signal from the implanted lead should be continuous and without artifact, similar to a body-surface ECG. A discontinuous signal may indicate a lead fracture or otherwise damaged lead, or an insulation break that would necessitate lead replacement. Inadequate signals may result in failure of the ICD system to detect an arrhythmia or in unnecessary delivery of therapy.

Conversion Testing

After obtaining acceptable signals, use the ICD pulse generator to demonstrate ability to reliably convert ventricular fibrillation (VF) and, when appropriate to the patient, ventricular tachycardias. This testing involves inducing arrhythmias and shocking the patient with high-voltage pulses delivered from the ICD pulse generator, through the defibrillation electrodes of the lead, to the heart.

CAUTION: Following an unsuccessful high-energy shock, miscounting of cardiac rate, delayed detection, or nondetection due to low amplitude VF signals, it may be necessary to reposition the lead or use a separate rate-counting electrode system. If a separate pace/sense electrode system is used, its interelectrode spacing must be no greater than 1-2 cm because greater separation may cause the signal from the leads to exceed the refractory period of the ICD pulse generator, resulting in oversensing in normal rhythm, or undersensing in polymorphic rhythm.

In addition, a wide pace/sense electrode separation may contribute to oversensing by introducing a large repolarization signal (T-wave), thereby causing false fulfillment of the rate criteria.

Reliable conversion of VF should be demonstrated at an energy level less than the maximum energy setting of the pulse generator. Boston Scientific recommends that multiple induction conversion tests of VF be performed to determine conversion reliability and the patient's defibrillation threshold (DFT). It is a matter of clinical judgment as to what constitutes a demonstration of reliable conversion. Since the result of any single test is subject to statistical variation, a one-time conversion of a rhythm disturbance at a particular energy level does not necessarily predict future conversion energy levels. Refer to the applicable ICD physician's manual for conversion testing guidelines.

Weigh the probability of reliable conversion in the ambulatory state against the availability of ICD energy settings and the patient's ability to tolerate multiple arrhythmia inductions.

If a patient's arrhythmia(s) cannot be reliably converted with an ENDOTAK RELIANCE or ENDOTAK RELIANCE SG lead, supplementary implantation an alternate lead system will require additional conversion testing.

WARNING: Use of any component of the ENDOTAK lead system to assist in delivery of external-source rescue shocks could cause extensive tissue damage.

The decision to implant any ICD lead system in any configuration should be based on demonstration of adequate safety margins at the programmed shock energy as determined by DFT and cardioversion energy requirement (CER) testing. Refer to the applicable ICD physician's manual for DFT and CER testing requirements.

Clinical study indicates that a programmed safety margin of 9–10 J above the patient's DFT was used in the majority of patients. If a 9–10 J safety margin cannot be obtained by other, less invasive means, consider placing an additional defibrillation lead.

Note: *If, after prolonged and repeated inductions of VF, a thoracotomy is to be performed, consider performing it at a later date.*

Securing the Lead

After the electrodes are satisfactorily positioned and conversion testing has been performed, secure the lead to the vein to achieve permanent hemostasis and lead stabilization. Suture sleeve tie-down techniques can vary with the lead insertion technique used. Securing the lead will provide permanent hemostasis and lead stabilization.

Percutaneous Implant Technique

1. Peel back the introducer sheath and slide the suture sleeve deep into the tissue (Figure 15).
2. Using both grooves, ligate the suture sleeve to the lead.

3. Next, secure the sleeve and lead to the fascia.

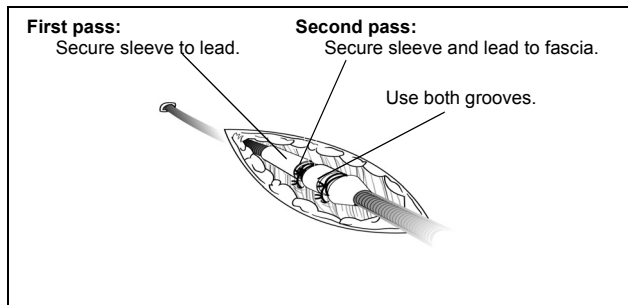


Figure 15. Using the sleeve with the percutaneous implant technique.

4. Check the suture sleeve after tie-down to demonstrate stability and lack of slippage by grasping the suture sleeve with fingers and trying to move the lead in either direction.

Venous Cut-Down Technique

1. Slide the suture sleeve into the vein past the distal pre-formed groove. Ligate the vein around the suture sleeve to obtain hemostasis. Next, using the same groove, secure the lead and vein to the adjacent fascia (Figure 16).

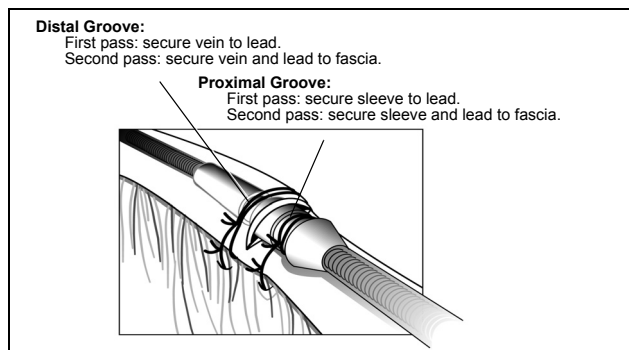


Figure 16. Using the sleeve with the venous cutdown technique.

2. Using the proximal pre-formed groove, secure the sleeve to the lead. Using the same groove, secure the sleeve and lead to the adjacent fascia.
3. Check the suture sleeve after tie-down to demonstrate stability and lack of slippage by grasping the suture sleeve with fingers and trying to move the lead in either direction.

WARNING: Do not kink, twist, or braid the lead terminal with other leads as doing so could cause lead insulation abrasion damage.

CAUTIONS:

- When ligating the vein, avoid too tight a stricture. A tight stricture might damage the silicone rubber insulation or sever the vein. Avoid dislodging the electrode tip during the anchoring procedure.
- Do not remove or cut the suture sleeves from the lead, as it may cause lead damage.

Abdominal Implants

Allow slack on the lead for strain relief on the lateral side of the suture sleeve near the venous entry site when securing the leads to body tissue (Figure 17). This will prevent lead dislodgment caused by the weight of the pulse generator or upper extremity movement.

Note: When implanting the lead via a subclavian puncture, allow slack in the lead between the distal suture sleeve and the venous entry site. This will help minimize flexing at the suture sleeve and interaction with the clavicle/first rib region.

Tunneling the Lead to the Abdominal Pocket

A short terminal leg (STL) tunneling tool is recommended for use with this lead if the ICD pulse generator is implanted in the abdomen. Tunnel the lead subcutaneously from the chest area to the abdominal ICD implant pocket. If the tunneling procedure must be delayed, cap the lead terminal pin and form a temporary pocket for the coiled lead. Capping the terminal pin protects it and prevents body fluids from entering the lumen of the lead.

Note: When using a Boston Scientific lead tunneler, do not cap the leads.

CAUTIONS:

- Tunnel the lead from the chest area to the pulse generator implant site. Never tunnel the lead from the pulse generator implant site to the chest area. This can damage the electrodes or lead body or both by permanently stretching the lead.
- When tunneling the lead, take precautions not to place excessive tension on the lead. This can cause either structural weakness or conductor discontinuity or both.

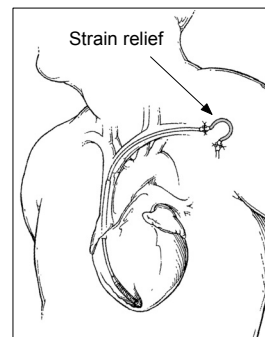


Figure 17. Position and shape of the strain relief loop.

- After tunneling, re-evaluate the lead to verify that no significant change in signals or damage to the lead has occurred during the tunneling procedure.

Reattach the lead terminals to the ICD pulse generator. If the measurements are unacceptable, check the electrical connections. A discontinuous or abnormal signal may indicate dislodgment, a loose connection, or lead damage. If necessary, reposition the lead electrodes until acceptable values are obtained. To reposition the lead, carefully withdraw the tunneled portion back to the venous entry site. Release the permanent ligatures and reposition the lead using procedures previously discussed.

Connection to a Pulse Generator

Consult the ICD physician's manual for directions concerning connecting the lead terminals to the pulse generator.

Verify the stylet is removed prior to connecting the lead to the pulse generator.

CAUTION: Insert the IS-1 lead terminal straight into the lead port. Do not bend the lead near the lead-header interface. Improper insertion can cause insulation damage near the terminal ring that could result in lead damage.

Notes:

- *If necessary, lubricate the lead terminal sparingly with sterile water to make insertion easier.*
- *If the lead terminal pin will not be connected to an ICD pulse generator at the time of lead implantation, the lead connector **must** be capped before closing the pocket incision. Place a suture around the lead cap to keep it in place.*
- *Plug any unused DF-1 lead port on the pulse generator with the DF-1 port plug (ENDOTAK RELIANCE SG lead only).*

The pace/sense terminal is inserted into the ICD lead port identified as the pacing/sensing port. The defibrillation terminals are inserted into the ICD lead ports identified as defibrillation, maintaining the polarity and electrode configuration determined during DFT testing.

Giving consideration to patient anatomy and pulse generator size and motion, gently coil any excess lead and place adjacent to the pulse generator. It is important to place the lead into the pocket in a manner that minimizes lead tension, twisting, sharp angles, and/or pressure.

Post-implant Evaluation

Perform follow-up evaluation as recommended in the applicable ICD pulse generator physician's manual.

CAUTION: For some patients, lead performance at implant may not predict performance in the chronic state. **Therefore, Boston Scientific strongly recommends that post-implant follow-up EP testing be performed before the patient is discharged from the hospital.** This testing should include at least one arrhythmia induction/conversion test of ventricular fibrillation.

In addition to the pulse generator follow-up instructions, use beeping tones to evaluate pacing/sensing integrity. If programmed accordingly, placing and holding a magnet over an active implanted pulse generator elicits tones synchronously with the R-wave of the pace/sense electrodes. If a problem exists with the pace/sense electrodes or their interface with the pulse generator, it may be revealed by evaluating the beeping tones of the device. Refer to the applicable ICD system manual for specific instructions.













Chronic repositioning of the lead may be difficult because of body fluid or fibrotic tissue intrusion into the helix mechanism.

Explantation

Return all explanted leads to Boston Scientific. Examination of explanted leads may provide information for continued improvement in system reliability. Use a Boston Scientific Returned Product Kit to properly package the lead and complete an Observation/Complication/Out-of-Service Report form. Send the form and kit to Boston Scientific at the address on the back of this manual.

Note: *Disposal of explanted devices is subject to local, state, and federal regulations. Contact your Boston Scientific representative or call Boston Scientific at 1-800-CARDIAC for a Returned Product Kit.*

SYMBOLS ON PACKAGING

Symbol	Definition
	Opening instructions
	Do not reuse
	Do not resterilize
	Consult instructions for use
	Sterilized using ethylene oxide
	Reference number
	Use by
	Date of manufacture
	Lot number
	Serial number
	Manufacturer
	Do not use if package is damaged

SPECIFICATIONS (Nominal)

	ENDOTAK RELIANCE SG	ENDOTAK RELIANCE G
Model and Length	0180–59 cm 0181–64 cm 0182–70 cm 0183–90 cm	0184–59 cm 0185–64 cm 0186–70 cm 0187–90 cm
Serial Numbers 299999 and Below: Expected number of rotations to fully extend/retract the helix ^a	0180, 0181, 0182–8 turns 0183–10 turns	0184, 0185, 0186–8 turns 0187–10 turns
Serial Numbers 300000 and Above: Expected number of rotations to fully extend/retract the helix ^a	0180, 0181, 0182–11 turns 0183–15 turns	0184, 0185, 0186–11 turns 0187–15 turns
Maximum number of rotations allowed to extend/retract the helix	0180, 0181, 0182–20 turns 0183–25 turns	0184, 0185, 0186–20 turns 0187–25 turns
Terminal sizes	(1) IS-1 bipolar, (1) DF-1	(1) IS-1 bipolar, (2) DF-1
Recommended lead introducer size		
Non-hemostatic introducer without guide wire	9F	9F
Non-hemostatic introducer with guide wire	10.5F	10.5F
Hemostatic introducer and TVI tool without guide wire	9.5F	9.5F
Hemostatic introducer and TVI tool with guide wire	11F	11F
Tip to proximal coil electrode length	NA	18 cm
Tip to distal coil electrode length	12 mm	12 mm
Maximum fixation helix penetration depth	1.9 mm	1.9 mm
Diameter:		
Insertion diameter	3.0 mm	3.0 mm
Isodiametric lead body	2.7 mm	2.7 mm
Coil electrode	2.7 mm	2.7 mm
Fixation Helix	1.3 mm	1.3 mm

32 | SPECIFICATIONS (Nominal)

Active surface area:		
Distal coil electrode	450 mm ²	450 mm ²
Proximal electrode	NA	660 mm ²
Active tip electrode	5.7 mm ²	5.7 mm ²
Material:		
External insulation	Silicone rubber	
DF-1 terminal pin	Titanium	
IS-1 terminal pin	Stainless steel	
Pace/sense conductor	MP35N nickel-cobalt alloy, PTFE sleeve	
Shocking conductor	Drawn brazed strand cable, PTFE coated	
Tip electrode (helix)	Platinum iridium	
Coil electrode covering	ePTFE	
Steroid	Approximately 1.0 mg dexamethasone acetate	
Compatibility	Boston Scientific ICD pulse generators	

- a. Use fluoroscopy markers for verification of full extension/retraction of helix.

Boston Scientific

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